

ORIGINAL RESEARCH

Open Access



Prediction of [^{177}Lu]Lu-DOTA-TATE therapy response using the absorbed dose estimated from [^{177}Lu]Lu-DOTA-TATE SPECT/CT in patients with metastatic neuroendocrine tumour

Sejin Ha¹, Yong-il Kim^{1,2*} , Jungsu S. Oh^{1,2}, Changhoon Yoo^{2,3}, Baek-Yeol Ryou^{2,3} and Jin-Sook Ryu^{1,2}

*Correspondence:
kyi821209@naver.com

¹ Department of Nuclear Medicine, Asan Medical Center, University of Ulsan College of Medicine, Seoul, Republic of Korea

² Theranostics Center, Asan Cancer Institute, Asan Medical Center, Seoul, Republic of Korea

³ Department of Oncology, Asan Medical Center, University of Ulsan College of Medicine, Seoul, Republic of Korea

Abstract

Background: Peptide receptor radionuclide therapy (PRRT) with [^{177}Lu]Lu-DOTA-TATE has shown efficacy in patients with metastatic neuroendocrine tumours (NETs). Personalised dosimetry is crucial to optimise treatment outcomes and minimise adverse events. In this study, we investigated the correlation between the tumour-absorbed dose (TAD) estimated from [^{177}Lu]Lu-DOTA-TATE SPECT/CT and the therapeutic response.

Method: A retrospective analysis was conducted on patients with advanced well-differentiated NETs grades 1–3 who underwent PRRT and exhibited greater uptake than liver on pre-therapeutic [^{68}Ga]Ga-DOTA-TOC PET/CT. Target lesions were selected based on the RECIST 1.1 and PERCIST 1.0 criteria using [^{177}Lu]Lu-DOTA-TATE SPECT/CT and pre-therapeutic contrast-enhanced CT scans. For anatomical image analysis, the sum of the longest diameter (SLD) of the target lesions was measured using the RECIST 1.1 criteria for patient-based analysis and the longest diameter (LD) of the target lesion using the RECIST-L criteria for lesion-based analysis. Standardised uptake values (SUVs) were measured on SPECT/CT images, and TADs were calculated based on the SUVs. Dosimetry was performed using a single SPECT/CT imaging time point at day 4–5 post-therapy. Statistical analyses were conducted to investigate correlations and determine the target lesion responses.

Results: Twenty patients with primary tumour sites and hepatic metastases were included. Fifty-five target lesions, predominantly located in the pancreas and liver, were analysed. The cumulative TAD (lesion-based analysis: $r = 0.299\text{--}0.301$, $p = 0.025\text{--}0.027$), but not the cycle 1 SUV (lesion-based analysis: $r = 0.198\text{--}0.206$, $p = 0.131\text{--}0.147$) or cycle 1 TAD (lesion-based analysis: $r = 0.209\text{--}0.217$, $p = 0.112\text{--}0.126$), exhibited a significant correlation with the change in LD of the target lesion. Binary logistic regression analysis identified the significance of the cumulative TAD in predicting disease control according to the RECIST-L criteria (odds ratio = 1.031–1.051, $p = 0.024\text{--}0.026$).

Conclusions: The cumulative TAD estimated from [^{177}Lu]Lu-DOTA-TATE SPECT/CT revealed a significant correlation with change in LD, which was significantly higher for the cumulative TAD than for the cycle 1 SUV or TAD. A higher cumulative TAD

was associated with disease control in the target lesion. However, considering the limitations inherent to a confined sample size, careful interpretation of these findings is required. Estimation of the cumulative TAD of [¹⁷⁷Lu]Lu-DOTA-TATE therapy could guide the platform towards personalised therapy.

Keywords: Neuroendocrine tumour, [¹⁷⁷Lu]Lu-DOTA-TATE, SPECT/CT, Dosimetry, Absorbed dose

Background

¹⁷⁷Lu-DOTA-0-Tyr3-Octreotate ([¹⁷⁷Lu]Lu-DOTA-TATE, Lutathera[®]) therapy, a peptide receptor radionuclide therapy (PRRT) targeting the somatostatin receptor (SSTR), is known to be effective in patients with metastatic neuroendocrine tumours (NETs) [1–5]. Personalised dosimetry of [¹⁷⁷Lu]Lu-DOTA-TATE therapy is potentially effective in maximising its therapeutic effects and minimising adverse events [6, 7]. [⁶⁸Ga]Ga-DOTA-TOC uptake is commonly used to assess the feasibility of PRRT and select suitable candidates by targeting SSTR [8]. Certain studies have indicated a notable link between pre-therapeutic [⁶⁸Ga]Ga-DOTA-TOC uptake and the absorbed dose in [¹⁷⁷Lu]Lu-DOTA-TATE therapy, suggesting that increased [⁶⁸Ga]Ga-DOTA-TATE uptake is associated with higher absorbed doses during [¹⁷⁷Lu]Lu-DOTA-TATE therapy. However, this relationship may not be robust enough for individualised dose planning [9, 10]. One study demonstrated a relatively strong correlation between the tumour-absorbed dose during [¹⁷⁷Lu]Lu-DOTA-TATE therapy and tumour reduction [11]. However, other studies have shown no significant correlation between the tumour-absorbed dose and tumour reduction [12, 13].

The absorbed dose of [¹⁷⁷Lu]Lu-DOTA-TATE by the tumour was originally estimated by performing 4 to 5 repeated sessions of [¹⁷⁷Lu]Lu-DOTA-TATE scintigraphy; however, this is too difficult to routinely perform in clinical practice. As an alternative, single-photon emission computed tomography/computed tomography (SPECT/CT) performed 4–5 days after PRRT can be used to accurately measure the absorbed dose of [¹⁷⁷Lu]Lu-DOTA-TATE by the tumour [14–16].

We hypothesised that the tumour-absorbed dose estimated from single SPECT/CT performed 4–5 days after PRRT could predict tumour response. In this study, we identified a correlation between the tumour-absorbed dose estimated from [¹⁷⁷Lu]Lu-DOTA-TATE SPECT/CT and the therapeutic response of the tumour according to the diameter changes on CT.

Methods

Patient selection

Between December 2019 and December 2021, a total of 32 patients with metastatic NETs who underwent PRRT were retrospectively evaluated. Patients were considered suitable for PRRT if they had advanced, well-differentiated NET grades 1–3, with more uptake than the liver on pre-therapeutic ⁶⁸Ga-DOTA-D-Phe1-Tyr3-Octreotide ([⁶⁸Ga]Ga-DOTA-TOC) positron emission tomography (PET)/CT (Krenning score ≥ 3 , on maximum intensity projection images) [17]. Patients who underwent [¹⁷⁷Lu]Lu-DOTA-TATE SPECT/CT 4–5 days after PRRT scans were included. Six patients without either

pre-therapeutic contrast-enhanced CT (CECT) or post-therapeutic CECT and three patients with intervals greater than 6 months between PRRTs were excluded from the study (Fig. 1). The other inclusion criteria were as follows: age > 18 years, Karnofsky performance status (KPS) \geq 70, estimated glomerular filtration rate (eGFR) > 40 mL/min, creatinine \leq 1.7 mg/dL, haemoglobin (Hb) > 8 g/dL, white blood cell (WBC) count > 2 000/ μ L, platelet count (PLT) > 70 000/ μ L, and total bilirubin < 3.0 mg/dL. This study was approved by our Institutional Review Board (IRB No. 2022-1581), and the requirement for informed consent was waived.

PRRT and SPECT/CT

Every 2–3 months, 7.4 GBq of [¹⁷⁷Lu]Lu-DOTA-TATE (Lutathera[®], Novartis, Switzerland) was intravenously injected up to four times [18]. Short- and long-acting somatostatin analogues were discontinued 24 h and 4 weeks before every treatment, respectively. On the day of therapy, patients were fasted for 4 h before and 2 h after PRRT. Two intravenous (IV) lines were inserted and vital signs and peripheral oxygen saturation (SpO₂) checked. The antiemetic drug ondansetron (Zofran[®]; GlaxoSmithKline, United Kingdom) was medicated 1–2 h before [¹⁷⁷Lu]Lu-DOTA-TATE infusion. Next, 1 000 mL of L-arginine 25 g/L-lysine 25 g (LysaKare[®]; Advanced Accelerator Applications, a Novartis company, France) was infused at a rate of 250 mL/h at least 30 min before initiation of [¹⁷⁷Lu]Lu-DOTA-TATE infusion. [¹⁷⁷Lu]Lu-DOTA-TATE was infused at a rate of 60 mL/h for approximately 30 min using a syringe pump. Patients were closely

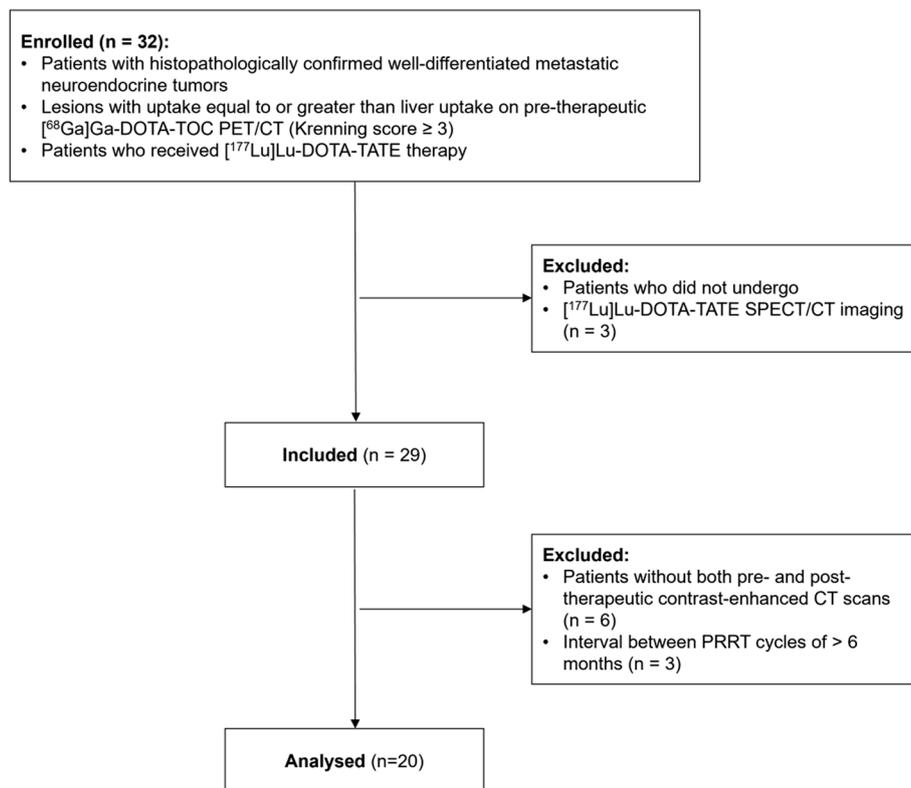


Fig. 1 Flow diagram of patient inclusion and exclusion

monitored during and for 4 h after PRRT to observe any acute side effects, including flushing, nausea, vomiting, diarrhoea, bronchospasm, hypertension, and carcinoid crisis. The patient's condition, including vital signs and SpO₂, was also recorded on a sheet every 30–60 min.

SPECT/CT imaging was performed 4–5 days after PRRT. Images were acquired using an integrated SPECT/CT scanner (Symbia Intevo; Siemens, Germany) equipped with medium-energy, low-penetration collimators from the neck to the proximal thigh area. The CT was acquired using the following parameters: 110 kVp, 40 ref mAs using adaptive dose modulation (CARE Dose 4D), 16 × 0.6 collimation, 1-s rotation time, 2-mm slice thickness, 2-mm increment, and 1 pitch. SPECT was acquired using the following parameters: 20% energy window centred at 208 keV, 256 × 256 matrices, 1.0 × zoom, 45 view, 22 s per view, and step-and-shoot mode. Image reconstruction was performed using an ordered subset conjugate gradient minimiser (OSCGM) algorithm (xSPECT; Siemens) with 24 iterations, 2 subsets, 5-mm Gaussian filter, and 256 × 256 matrices, enabling the quantification of SPECT/CT images. Our SPECT/CT camera utilized Siemens xSPECT software capable of producing SUV images, unlike traditional SPECT images that display counts, thereby enhancing the accuracy of our dosimetry study.

Target lesion selection

Target lesions were selected according to the RECIST 1.1 and practical PERCIST 1.0 criteria [19–21]. Tumours with the hottest uptake on [¹⁷⁷Lu]Lu-DOTA-TATE SPECT/CT with > 10 mm in the longest diameter on pre-therapeutic CECT scan were selected. Up to five tumours per patient and up to two tumours per organ were analysed. Bone metastases were excluded because the diameter change of bone metastases cannot be appropriately evaluated with CECT [22–25].

Anatomical image analysis

The longest diameter of the target lesion was measured on pre- and post-therapeutic CECT and averaged by two experienced nuclear medicine physicians (S.J.H. and Y.I.K.) who were blinded to the clinical and SPECT/CT data. Pre-therapeutic CECT scans were performed within 3 months prior to cycle 1 PRRT, with a median of 29 days (range: 3–74 days). Post-therapeutic CECT scans were performed within 3 months after the final PRRT cycle, with a median of 30 days (range: 2–71 days). Changes in the diameters of target lesions were measured and evaluated by patient-based and lesion-based according to the RECIST 1.1 and RECIST-L criteria, respectively [20].

1. RECIST 1.1 (patient-based) criteria: disappearance of the target lesion was defined as 'complete response', decrease in the sum of the longest diameters (SLD) of the target lesions $\geq 30\%$ was defined as 'partial response', increase in the SLD of the target lesions $\geq 20\%$ was defined as 'progression', and in between was defined as 'stable disease'.
2. RECIST-L (lesion-based) criteria: disappearance of the target lesion was defined as 'complete response', decrease in the longest diameter (LD) of the target lesion $\geq 30\%$ was defined as 'partial response', increase in the longest diameter of the target

lesion $\geq 20\%$ was defined as ‘progression’, and in between was defined as ‘stable disease’.

Disease control was defined as ‘partial response’ or ‘stable disease’. Both patient-based and lesion-based analyses were performed.

Standardised uptake value (SUV) measurement

The SUVs of target lesions were measured on SPECT/CT images 4–5 days after treatment with [^{177}Lu]Lu-DOTA-TATE using Mirada DBX software (version 1.2.0.59; Mirada Medical, Ltd., Oxford, United Kingdom) [26–28]. SUV_{max} was defined as the voxel with the highest uptake on SPECT/CT within the volume-of-interest (VOI) of RECIST 1.1-selected lesions. The SUV_{peak} was defined as the maximum average SUV within a 1-cm^3 sphere. The SUV_{41} was defined as the mean SUV of all voxels with an activity of 41–100% of the voxel with the highest uptake (SUV_{max}) within the VOI. The SUV_{41} was calculated by adjusting the iso-contour, which was automatically delineated using 41% of SUV_{max} within the VOI [29]. Most target lesions were automatically delineated; nevertheless, a few VOIs of the target lesions required manual correction to exclude other closely located tumour lesions.

Tumour-absorbed dose (TAD)

Based on a study by Hanscheid et al. [14], we used the SUV_{max} , SUV_{peak} , and SUV_{41} of target lesions measured on SPECT/CT taken 4–5 days after PRRT by converting them to Dose_{max} , $\text{Dose}_{\text{peak}}$, and Dose_{41} , respectively. Unlike Hanscheid et al., who formulated the absorbed dose in terms of counts in the VOI, we formulated the absorbed dose in terms of SUV as follows:

The equation used by Hanscheid et al. can be rephrased as [14]:

$$D[\text{Gy}] = 0.25 \left[\text{Gy} \frac{\text{g}}{\text{MBqh}} \right] t1[\text{h}] \text{VOIAC} \left[\frac{\text{MBq}}{\text{g}} \right]$$

Since it is well known that:

$$\text{SUV} = \frac{\text{VOIAC} \left[\frac{\text{MBq}}{\text{g}} \right] \text{BW}[\text{g}] 2^{\frac{t1}{T_{1/2}}}}{\text{ID}[\text{MBq}]}$$

We rephrased the dose equation in terms of VOI counts. Finally, the max/peak/mean dose in the VOI using max/peak/mean SUVs was:

$$D[\text{Gy}] = 0.25 \left[\text{Gy} \frac{\text{g}}{\text{MBqh}} \right] t1[\text{h}] \frac{\text{SUVID}[\text{MBq}]}{\text{BW}[\text{g}] 2^{\frac{t1}{T_{1/2}}}}$$

where D is TAD, VOIAC stands for VOI activity concentration, $t1$ is SPECT/CT acquisition time from injection [h], BW is body weight [g], ID is the injected dose [MBq], and $T_{1/2}$ is the half-life of ^{177}Lu [h]. Notably, the dose was based on decay-uncorrected VOI counts, whereas SUV was based on decay-corrected VOI counts. In addition, we also

employed the assumptions of the OLINDA unit-density sphere model and no cross dose between organs as conducted by Hanscheid et al. [14].

The cumulative tumour-absorbed $Dose_{max}$, $Dose_{peak}$, and $Dose_{41}$ were defined as the sum of the tumour-absorbed $Dose_{max}$, $Dose_{peak}$, and $Dose_{41}$ from all PRRT cycles, respectively. The cut-off values of the cumulative tumour-absorbed $Dose_{max}$, $Dose_{peak}$, and $Dose_{41}$ to achieve disease control were checked for all target lesions.

Inter-cyclic changes in TAD

The ratio of the TAD between PRRT cycles ($R_{N,M}$) was calculated as follows:

$R_{N,M}$ (%) = 100 (TAD from PRRT cycle M /TAD from PRRT cycle N) ($N=1-3$, $M=2-4$, $M>N$). The TADs estimated from target lesions with all four cycles of PRRT and SPECT/CT were used to calculate the inter-cyclic changes. Inter-cyclic changes of TAD were used to extrapolate missing SUV data.

Statistical analysis

Commercially available software, SPSS for Windows (version 21.0; IBM, Chicago, USA), was used to conduct statistical analyses. The correlations between diameter change of the target lesion (%) and the cycle 1 SUV, cycle 1 TAD, and cumulative TAD were evaluated using the Pearson correlation coefficient (r). Fisher z transformation was performed to compare correlation coefficients. The target lesion response was divided into two categories, namely disease control and disease progression, and a binary logistic regression method was used to explain the relationship between the TAD and target lesion response. A p -value < 0.05 was considered statistically significant.

Results

Patients and PRRT

Finally, 20 patients [6 men and 14 women; mean \pm standard deviation (SD) age: 57.5 ± 9.6 years, range: 34–75 years] were included in this retrospective study. The primary tumour sites were the pancreas, rectum, duodenum, stomach, kidney, and unknown in 10, 6, 1, 1, 1, and 1 patients, respectively. Hepatic metastases were detected in all patients. Among the extrahepatic metastases, lymph node metastases, bone metastases, peritoneal seeding, and other metastases were detected in 15, 11, 3, and 5 patients, respectively. The Ki-67 index of histopathologically confirmed tumours was $\leq 2\%$, 3–20%, and $> 20\%$ in 1, 15, and 4 patients, respectively. The Krenning scores of tumours with the most intense uptake on pre-therapeutic [^{68}Ga]Ga-DOTA-TOC PET/CT were three in six patients and four in 14 patients. Among the 55 target lesions, 7, 37, 10, and 1 target lesions were in the pancreas, liver, lymph node, and peritoneal seeding, respectively. All patients received at least two cycles of PRRT; however, most received four. The interval between PRRT cycles was 71 ± 19 days (range: 49–151 days). The patient characteristics are summarised in Table 1. Most patients (85%) did not receive other treatments, except for short-acting somatostatin analogue approximately 1 month before and after PRRT. However, three patients (15%) received everolimus and PRRT concomitantly (Table 2). SPECT/CT imaging was not performed in six out of 75 PRRT cycles for different patients. Thirteen SUV data from different target lesions could not be measured as these data were extrapolated using inter-cyclic changes between PRRT cycles. The

Table 1 Patient demographics and baseline clinical characteristics ($n = 20$)

Variables	Values
Age at diagnosis (years)	57.5 ± 9.6 [34–75]
Sex (male/female)	6:14
Primary tumour site, n (%)	
Pancreas	10 (50%)
Rectum	6 (30%)
Duodenum	1 (5%)
Stomach	1 (5%)
Kidney	1 (5%)
Unknown	1 (5%)
Hepatic metastasis, n (%)	20 (100%)
Extrahepatic metastasis, n (%)	18 (90%)
Lymph node	15 (75%)
Bone	11 (55%)
Peritoneal seeding	3 (15%)
Other	5 (25%)
Grade, n (%)	
1	1 (5%)
2	15 (75%)
3	4 (20%)
Ki-67, n (%)	
< 3%	1 (0.7%)
3–20%	15 (9.5% ± 4.8%)
> 20%	4 (25.3% ± 3.3%)
Krenning score, n (%)	
3	6 (30%)
4	14 (70%)
Site of target lesions, n	55
Pancreas	7
Liver	37
Lymph node	10
Peritoneal seeding	1
Number of PRRT cycles, n (%)	
1	0 (0%)
2	2 (10%)
3	1 (5%)
4	17 (85%)
Interval between PRRT cycles (days)	71 ± 19 [49–151]

SD: standard deviation, PRRT: peptide receptor radionuclide therapy

detailed number of target lesions and SUV data are listed in Additional file 1: Table S1, and the volumes of the target lesions are listed in Additional file 1: Table S2.

Cyclic changes in the TAD

Cyclic changes in the TAD were calculated using 34 target lesions from 12 patients who received all four cycles of PRRT after correction for administered [^{177}Lu]Lu-DOTA-TATE activity. The TAD tends to decrease gradually after each PRRT cycle. The cyclic changes in the TAD are summarised in Additional file 1: Table S3.

Table 2 Patient treatment other than PRRT ($n = 20$)

Treatment	Number of patients, n (%)
Previous treatment	
Surgery	11 (55%)
Liver-directed treatment	5 (25%)
RFA	2 (10%)
TACE	3 (15%)
Somatostatin analogue	13 (65%)
Cytotoxic chemotherapy	14 (70%)
Everolimus	16 (80%)
Concomitant treatment	
Everolimus	3 (15%)

RFA: radiofrequency ablation, TACE: transarterial chemoembolization

TAD and diameter change of the target lesion relationship

The SLD of target lesions on pre-therapeutic CT was 104.2 ± 54.9 mm (range between the 25th and 75th percentiles: 69.5–128.4 mm). The change in the SLD of target lesions was 17.7 ± 28.4 mm (range between the 25th and 75th percentiles: 7.5–32.1 mm) and $12.6\% \pm 32.2\%$ (range between the 25th and the 75th percentiles: 5.6%–31.1%). The median cumulative TAD_{max}, TAD_{peak}, and TAD₄₁ of the patients were 127.5 Gy (range between the 25th and 75th percentiles: 70.9–190.6 Gy), 113.9 Gy (range between the 25th and 75th percentiles: 64.4–171.9 Gy), 77.9 Gy (range between the 25th and 75th percentiles: 43.4–117.7 Gy), respectively.

The LD of the target lesion on pre-therapeutic CT was 37.9 ± 20.6 mm (range between the 25th and 75th percentiles: 24.0–44.7 mm). The diameter change of the target lesion was 6.4 ± 12.1 mm (range between the 25th and 75th percentiles: 2.8–13.3 mm) and $15.2\% \pm 29.4\%$ (range between the 25th and 75th percentiles: 7.9%–31.2%). The cumulative TAD_{max}, TAD_{peak}, and TAD₄₁ of the total lesions were 122.4 Gy (range between the 25th and 75th percentiles: 63.0–181.7 Gy), 112.3 Gy (range between the 25th and 75th percentiles: 56.1–166.2 Gy), and 70.6 Gy (range between the 25th and 75th percentiles: 37.3–111.3 Gy), respectively. Details regarding the cycle 1 and cumulative TADs of the target lesions based on patient-based and lesion-based analyses are summarised in Table 3.

Based on the RECIST 1.1 criteria, 7, 11, and 2 patients were classified as partial response, stable disease, and progressive disease, respectively. Based on the RECIST-L criteria, 15, 33, and 7 target lesions were classified as partial response, stable disease, and progressive disease, respectively (Table 4).

Neither the cycle 1 SUV nor the cycle 1 TAD was significantly correlated with changes in the SLD or LD of the target lesion (%). The cumulative TAD_{max} ($r = 0.428$, $p = 0.060$), TAD_{peak} ($r = 0.419$, $p = 0.066$), and TAD₄₁ ($r = 0.424$, $p = 0.063$) were moderately correlated with changes in the SLDs of target lesions, however, these correlations were not statistically significant. The cumulative TAD_{max} ($r = 0.301$, $p = 0.025$), TAD_{peak} ($r = 0.299$, $p = 0.026$), and TAD₄₁ ($r = 0.299$, $p = 0.027$) were weakly correlated with changes in the LD of target lesions with significance (Table 5). On comparing the r values using Fisher's

Table 3 Cycle 1 and cumulative TADs of the target lesions

	Per-patient	Total lesion	Pancreas	Liver	Lymph node
Cycle 1 TAD _{max} (Gy)	42.3 [5.5–120.3] IQR: 21.9–76.4	38.9 [3.7–179.5] IQR: 19.8–69.8	32.7 [8.6–84.8] IQR: 23.1–59.2	46.5 [3.7–179.5] IQR: 32.5–79.1	19.7 [12.2–38.9] IQR: 15.0–26.6
Cycle 1 TAD _{peak} (Gy)	38.2 [5.0–108.6] IQR: 19.9–69.5	33.7 [3.3–167.1] IQR: 17.9–64.3	30.2 [7.5–78.8] IQR: 21.6–55.4	41.6 [3.3–167.1] IQR: 27.3–73.5	17.4 [10.9–33.7] IQR: 13.6–23.8
Cycle 1 TAD ₄₁ (Gy)	26.1 [3.6–74.8] IQR: 13.2–46.8	23.8 [2.3–110.5] IQR: 12.5–42.7	18.6 [5.7–47.5] IQR: 14.8–35.3	28.4 [2.3–110.5] IQR: 19.6–44.5	12.5 [7.6–23.8] IQR: 9.4–16.4
Cumulative TAD _{max} (Gy)	127.5 [36.6–271.9] IQR: 70.9–190.6	122.4 [17.6–329.7] IQR: 63.0–181.7	110.3 [26.0–234.9] IQR: 69.1–179.9	149.6 [17.6–329.7] IQR: 91.2–214.8	55.6 [28.8–90.0] IQR: 44.7–69.5
Cumulative TAD _{peak} (Gy)	113.9 [33.8–253.7] IQR: 64.4–171.9	112.3 [14.5–298.2] IQR: 56.1–166.2	101.3 [23.3–217.8] IQR: 64.1–166.2	132.4 [14.5–298.2] IQR: 86.4–187.9	48.3 [26.9–79.3] IQR: 40.0–61.2
Cumulative TAD ₄₁ (Gy)	77.9 [23.8–170.2] IQR: 43.4–117.7	70.6 [10.9–208.7] IQR: 37.3–111.3	62.9 [16.2–142.0] IQR: 43.2–107.3	91.0 [10.9–208.7] IQR: 57.9–130.2	34.4 [18.2–55.5] IQR: 28.3–42.0

Median [Range]

TAD: tumour-absorbed dose, IQR: interquartile range,

Per-patient: weighted average of the TADs of the target lesions in every patient, Cumulative TAD: sum of the TADs from all PRRT cycles

Table 4 Patient response summary and target lesions

	Response		
	Partial response, <i>n</i>	Stable disease, <i>n</i>	Progressive disease, <i>n</i>
Overall patients (<i>n</i> = 20)	7	11	2
Total lesion (<i>n</i> = 55)	15	33	7
Pancreas (<i>n</i> = 7)	0	5	2
Liver (<i>n</i> = 37)	12	22	3
Lymph node (<i>n</i> = 10)	3	5	2
Peritoneal seeding (<i>n</i> = 1)	0	1	0

z transformation, none of the results were statistically significant. A subgroup analysis without the outlier (a patient with a diameter change of target lesion – 103%), demonstrating similar results, is presented in Additional file 1: Table S4.

Patient- and lesion-based scatter plots of the cumulative TAD against the diameter change of the target lesion are shown in Figs. 2 and 3, respectively. The change in the LD of the target lesion exceeded –20% (‘disease control’ state according to the RECIST-L criteria) when the cumulative Dose_{max}, Dose_{peak}, and Dose₄₁ were ≥ 107.4, 93.7, and 65.4 Gy, respectively (Fig. 3).

Binary logistic regression analysis was performed to determine the relationship between the cycle 1 SUV, cycle 1 TAD, and cumulative TAD and disease control according to the RECIST 1.1 or RECIST-L criteria. The only statistically significant odds ratio observed was between the cumulative TAD and disease control, as per the RECIST-L criteria. Based on the RECIST-L criteria, the probability of disease control increased by 3.1% [95% confidence interval (CI): 0.4%, 5.9%], 3.4% (95% CI: 0.4%, 6.6%), and 5.1% (95% CI: 0.6%, 9.8%) as the cumulative TAD_{max}, TAD_{peak}, and TAD₄₁ increased by 1 Gy, respectively (Table 6). A representative case of partial response is presented in Fig. 4.

Table 5 Correlation analyses of cycle 1 SUVs, cycle 1 TADs, and cumulative TADs with diameter change (%)

	<i>r</i> (patient-based)	<i>p</i> (patient-based)	Durbin-Watson (patient-based)	<i>r</i> (lesion-based)	<i>p</i> (lesion-based)	Durbin-Watson (lesion-based)
Cycle 1 SUV _{max}	0.313	0.178	1.483	0.198	0.147	1.866
Cycle 1 SUV _{peak}	0.316	0.175	1.486	0.206	0.131	1.869
Cycle 1 SUV ₄₁	0.313	0.178	1.476	0.201	0.141	1.867
Cycle 1 TAD _{max} (Gy)	0.327	0.160	1.527	0.209	0.126	1.86
Cycle 1 TAD _{peak} (Gy)	0.332	0.153	1.532	0.217	0.112	1.863
Cycle 1 TAD ₄₁ (Gy)	0.326	0.161	1.519	0.21	0.123	1.861
Cumulative TAD _{max} (Gy)	0.428	0.060	1.668	0.301	0.025*	1.866
Cumulative TAD _{peak} (Gy)	0.419	0.066	1.658	0.299	0.026*	1.873
Cumulative TAD ₄₁ (Gy)	0.424	0.063	1.653	0.299	0.027*	1.869

SUV: standardised uptake value, TAD: tumour-absorbed dose

Cumulative TAD: sum of the tumour-absorbed doses from all PRRT cycles

A subgroup analysis without the outlier is presented in Additional file 1: Table S4

* $p < 0.05$

Discussion

Our research demonstrated a significant correlation between the cumulative TAD and percentage changes in LD of the target lesion [30]. The correlation between the cumulative TAD and percentage changes in the SLD of the patient was moderate but not statistically significant. There was no significant correlation between the LD of the target lesion and the cycle 1 SUV or TAD. The analysis excluding outliers similarly indicated a significant correlation only between the cumulative TAD and the percentage changes in the LD of the target lesion. Binary logistic regression analysis showed that an increase in the cumulative TAD would lead to a greater chance of disease control based on the RECIST-L criteria.

In our study, every target lesion achieved disease control when the cumulative TAD_{max}, cumulative TAD_{peak}, and cumulative TAD₄₁ were not < 107.4, 93.7, and 65.4 Gy, respectively. These cumulative TADs of target lesions could serve as potential threshold values to anticipate favourable treatment responses during PRRT. However, it should be noted that only two out of 20 patients in our study cohort did not achieve disease control.

On analysing the correlation between cycle 1 TADs and cumulative TADs, R^2 ranged from 0.77 to 0.79 (strong correlation; cycle 1 TAD_{max} vs. cumulative TAD_{max}: $R^2 = 0.78$, cycle 1 TAD_{peak} vs. cumulative TAD_{peak}: $R^2 = 0.79$, cycle 1 TAD₄₁ vs. cumulative TAD₄₁: $R^2 = 0.78$), implying that cycle 1 TADs could not be used to fully estimate cumulative TADs. In contrast, R^2 between cumulative TADs ranged from 0.99 to 1.00 (almost perfect correlation; cumulative TAD_{max} vs. cumulative TAD_{peak}: $R^2 = 1.00$, cumulative TAD_{max} vs. cumulative TAD₄₁: $R^2 = 0.99$, cumulative TAD_{peak} vs. cumulative TAD₄₁: $R^2 = 1.00$), indicating no significant change between cumulative TAD parameters. Moreover, consistent administration of 7.4 GBq in each PRRT cycle resulted in an observed

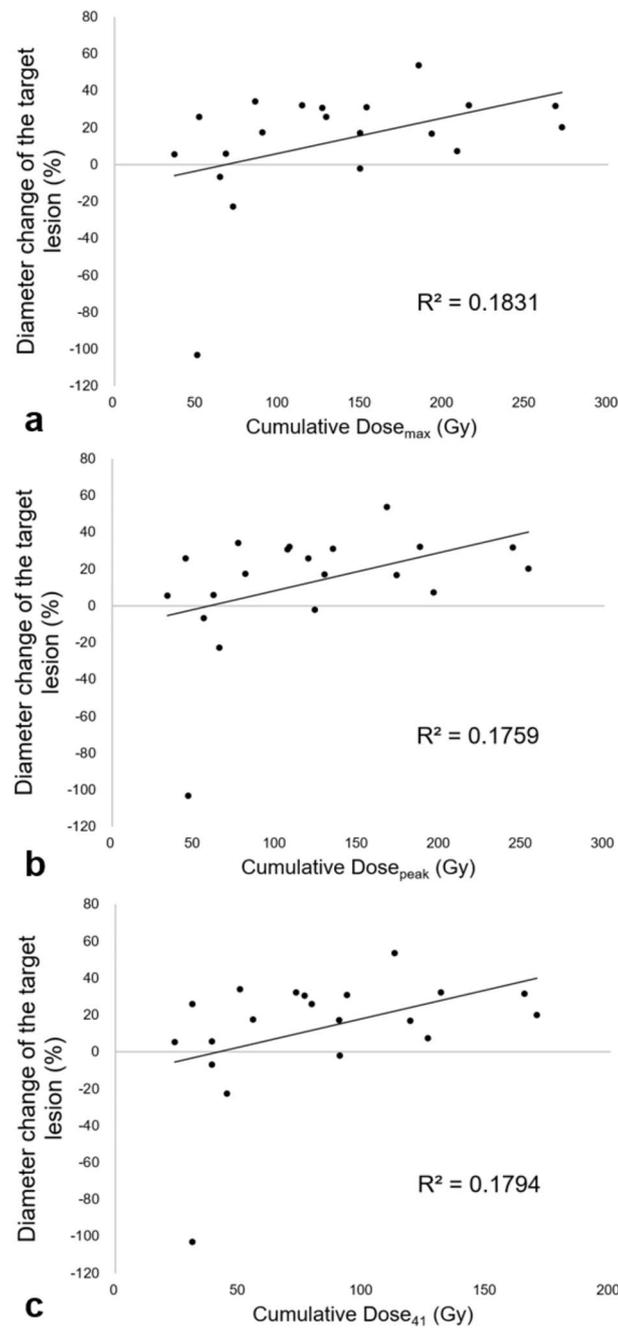


Fig. 2 Patient-based scatter plots of the cumulative tumour-absorbed dose (TAD) against the diameter change of the target lesion (%). **A** Cumulative TAD_{max}, **B** Cumulative TAD_{peak}, and **C** Cumulative TAD₄₁

decline in the median TAD over successive cycles. This observation suggests that even when SUVs with comparable intensities are evident in [⁶⁸Ga]Ga-DOTA-TOC PET/CT and [¹⁷⁷Lu]Lu-DOTA-TATE SPECT/CT across different PRRT cycles, the estimated TAD is potentially reduced in subsequent cycles. Based on these findings, a higher dose of radiotracer, within the patient's tolerance range, during the initial cycles may enhance therapeutic efficacy.

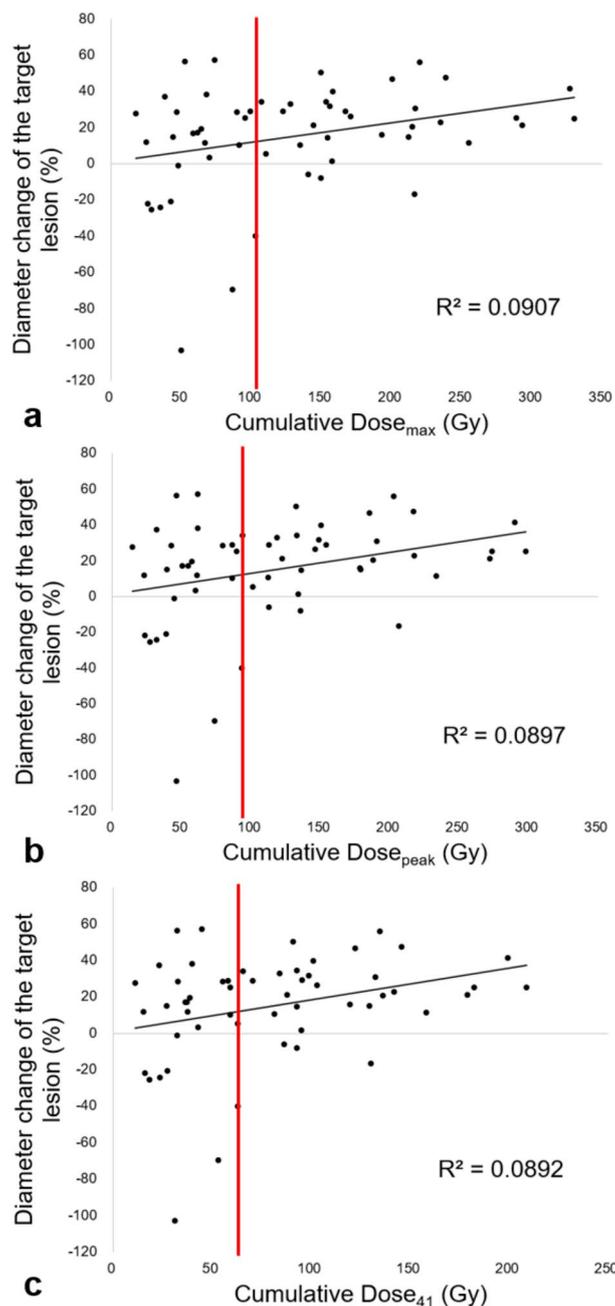


Fig. 3 Lesion-based scatter plots of the cumulative tumour-absorbed dose (TAD) against the diameter change of the target lesion (%). **A** Cumulative TAD_{max}: Diameter change (%) of the target lesion was > -20% (disease control state according to RECIST 1.1 criteria) when the cumulative dose was ≥ 107.4 Gy (vertical red line). **B** Cumulative TAD_{peak}: Diameter change (%) of the target lesion was > -20% (disease control state according to RECIST criteria) when the cumulative dose was ≥ 93.7 Gy (vertical red line). **C** Cumulative TAD₄₁: Diameter change (%) of the target lesion was > -20% (disease control state according to RECIST criteria) when the cumulative dose was ≥ 65.4 Gy (vertical red line)

On comparing our study to previous studies on the dosimetry and/or dose-response relationship of [¹⁷⁷Lu]Lu-DOTA-TATE treatment, not only our study but also most other studies, except for that by Ilan et al. [11], were retrospective in nature [12, 13, 31–33]. Notably, Ilan et al. [11], Jahn et al. [12], Jahn et al. [31], and Roth

Table 6 Binary logistic regression analyses between cumulative TADs and target lesion response based on RECIST-L criteria

Dependent variable	Independent variable	Odds ratio [confidence interval]	<i>p</i>
Disease control (RECIST-L)	Cumulative TAD _{max}	1.031 [1.004, 1.059]	0.024*
	Cumulative TAD _{peak}	1.034 [1.004, 1.066]	0.025*
	Cumulative TAD ₄₁	1.051 [1.006, 1.098]	0.026*

TAD: tumour-absorbed dose

Cumulative TAD: sum of the tumour-absorbed doses from all PRRT cycles

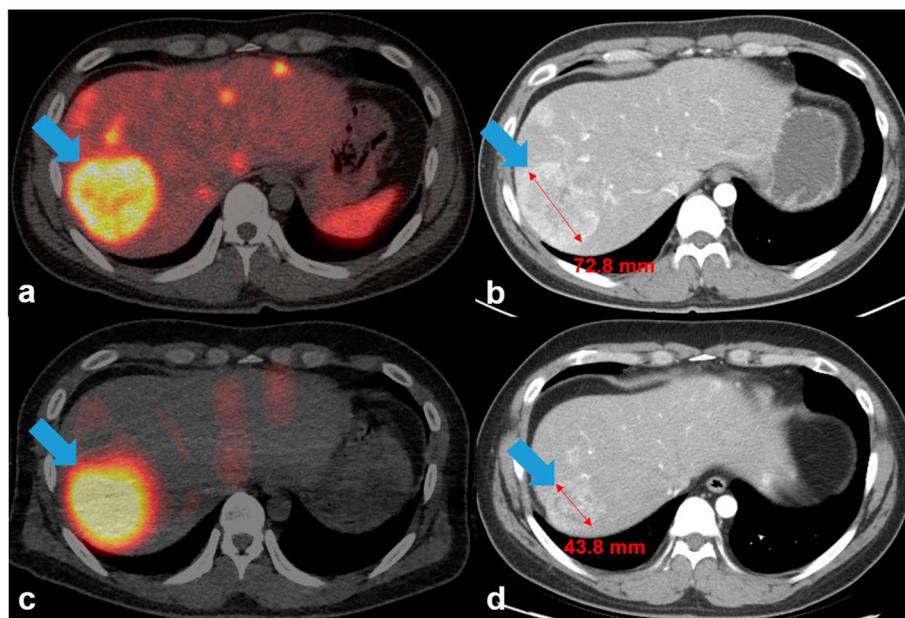
* *p* < 0.05

Fig. 4 Representative images of the patient's target lesion (liver) following ^{177}Lu Lu-DOTA-TATE therapy, showing a partial response (arrows). **A** Pre-therapeutic ^{68}Ga Ga-DOTA-TOC PET/CT exhibited a target lesion uptake in the liver that was more intense than normal liver uptake (Krenning score 3). **B** The lesion's largest diameter measured 72.8 mm on pre-therapeutic CECT. After four cycles of ^{177}Lu Lu-DOTA-TATE therapy, **C** ^{177}Lu Lu-DOTA-TATE SPECT/CT, captured after the fourth PRRT cycle (SPECT/CT images after PRRT cycles 1–3 are not shown), revealed target lesion uptake in the liver that was more intense than normal liver uptake (Krenning score 3). The cumulative tumour-absorbed Dose_{max}, Dose_{peak}, and Dose₄₁ of the target lesions were 157.8, 150.7, and 101.2 Gy, respectively. Following PRRT, the target lesion's longest diameter decreased by > 30%, measuring 43.8 mm on **(D)** post-therapeutic CECT

et al. [32] specifically included tumours of sizes larger than a certain diameter or volume in their analyses to mitigate the partial volume effect, whereas our study and that by Alipour et al. [33] did not. Ilan et al. [11], Jahn et al. [12], and Jahn et al. [31] used evaluation criteria based on the 'best response'. Conversely, Del Prete et al. [13] and Alipour et al. [33] did not use the 'best response' as their criterion. Jahn et al. [12] indicated a slightly weaker lesion-based correlation of $R^2 = 0.16$ than that in our study, terming it 'borderline'. A study by Ilan et al. [11] demonstrated a strong lesion-based correlation for lesions with diameters > 2.2 cm ($R^2 = 0.64$) and > 4 cm ($R^2 = 0.91$). Jahn et al. [31] further categorised their findings by lesion type, revealing that pancreatic neuroendocrine neoplasms had a correlation of $R^2 = 0.37$, while small

intestine neuroendocrine neoplasms had $R^2 = 0.29$. Del Prete et al. [13] and Alipour et al. [33] found no significant correlation between dose and volume. The results of the relationship between the TAD and tumour response are potentially affected by various factors, including neuroendocrine neoplasm type and evaluation method, that is, whether it is based on diameter or volume change or whether it uses the 'best response' criterion. Comparisons with previous studies on the dose–response relationship can be found in Additional file 1: Table S5.

Regarding the absorbed dose, the median total lesion cycle 1 TAD₄₁ determined in our study was 23.8 Gy (range: 2.3–110.5 Gy) with interquartile range of 12.5–42.7 Gy. In comparison, Ilan et al. [11] reported the most frequent cycle 1 TAD values around 20 Gy, with a median of 50 Gy (range: 10–170 Gy). Jahn et al. [12] reported a median cycle 1 TAD of 33.51 Gy (range: 11.24–108.5 Gy), with interquartile range of 23.2–51.1 Gy. Roth et al. [32] reported median cycle 1 TADs of 33 Gy for grade 1 tumours and 27 Gy for grade 2 tumours. Lastly, Alipour et al. [33] reported a median cycle 1 TAD of 29 Gy (range: 5–135 Gy) for measurable lesions, using single time point dosimetric measurement (at 24-h post-therapy). There are no significant differences between the cycle 1 TAD values of previous studies and those of our study.

We chose not to discard missing SUV data and instead extrapolated these using inter-cycle changes between PRRT cycles; this approach is more applicable to real-world situations where performing SPECT/CT may not always be feasible. We encountered cases where SPECT/CT was not performed due to various circumstances, such as a patient's poor condition or personal schedule, leading to 13 cases of unmeasurable SUV data. To address this issue, we calculated the inter-cycle changes in TAD, which we then used to extrapolate the missing SUV data, although the ratio between TADs in the initial and final PRRT cycles may vary by tumour type [31, 34]. We observed a steady decline in the median TAD following each PRRT cycle, consistent with the findings of previous studies [31–33]. While Jahn et al. did not specify any declining values [31], our study found a median TAD₄₁ decrease of 14.9–19.8% per cycle. This rate is in line with the reported decline of 14% per cycle for grade 2 tumours by Roth De et al. [32] and 18–25.8% per cycle for grade 1–3 tumours by Alipour et al. [33]. Notably, 61% of the tumours in the study by Alipour et al. [33] were grade 2, which is comparable to our study, where most patients (75%) were classified as grade 2.

We evaluated up to five target lesions per patient according to the RECIST 1.1 and practical PERCIST 1.0 guidelines and conducted both patient-based and lesion-based analyses. Some studies simplify their design by selecting a single target lesion with the highest uptake per patient when using [⁶⁸Ga]Ga-DOTA-TOC PET/CT to evaluate the treatment response of [¹⁷⁷Lu]Lu-DOTA-TATE [35]. However, considering the inherent heterogeneity of NETs, the evaluation of multiple lesions per patient would provide a more comprehensive reflection of tumour characteristics [36].

The TAD was generally thought to be estimated from the SUV_{mean} (in our study, the cumulative TAD₄₁); however, our study yielded similar results for the cumulative TAD_{max} and cumulative TAD_{peak}. As the cumulative TAD_{max} and cumulative TAD_{peak} offer the advantage of simple and reproducible measurements without the need for specific software, such as MIRADA, for assessment, these parameters could be widely applied in future studies.

A SPECT/CT schedule of 4–5 days after PRRT is preferable for patient convenience compared with that of 7 days. However, some reports have suggested that the absorbed dose conversion using 7-day data is more accurate than that using 4–5-day data [14, 15, 37]. Further studies would be needed to compare the TAD using 4–5- and 7-day post-PRRT data.

The median time interval of 30 days (range: 2–71 days) between the final PRRT cycle and post-therapeutic CT in our study was relatively short compared with prior reports of response assessment. This short interval could increase the possibility of pseudo-progression and the underestimation of tumour diameter changes. However, some patients' early follow-up CT were necessitated by their clinical circumstances. For example, a patient with a –22.8% change in diameter (who demonstrated disease progression) underwent follow-up CT only 2 days after the last PRRT cycle due to our clinical suspicion of disease progression.

Several limitations should be considered when applying the results of this study to real-world scenarios. First, this study followed a retrospective design and was conducted using a small cohort. Therefore, the results should not be over-emphasised. In addition, 11 out of 20 patients were diagnosed with bone metastases; however, bone lesions were not considered target lesions in our study. However, it is widely recognised that evaluating treatment response by measuring changes in target lesion size on CT scans has limitations [38]. Furthermore, as we did not use partial volume effect correction methods [39], the mean TAD could have been underestimated. Finally, we were unable to analyse the correlation between the disease control status of target lesions and clinical outcomes, such as mortality. Therefore, further research is required to explore the clinical significance and implications of our findings.

Conclusions

The cumulative TAD estimated from [¹⁷⁷Lu]Lu-DOTA-TATE SPECT/CT conducted 4–5 days after PRRT demonstrated significant correlations with changes in the LD of the target lesion in per-lesion analyses. These correlations with the cumulative TAD were found to be stronger than that with the cycle 1 SUV or TAD. Furthermore, a higher cumulative TAD was associated with a higher likelihood of disease control in the target lesion. Notably, cumulative TAD_{max} showed a correlation that was at least as robust as cumulative TAD_{peak} and cumulative TAD₄₁, suggesting its potential use as a convenient and valuable parameter for predicting tumour response after PRRT. Nonetheless, considering the constraints of the limited sample in this study, a cautious approach to these results is advised.

Abbreviations

DOTA-TATE	DOTA-0-Tyr3-Octreotate
PRRT	Peptide receptor radionuclide therapy
SSTR	Somatostatin receptor
NET	Neuroendocrine tumour
SPECT	Single-photon emission computed tomography
CT	Computed tomography
DOTA-TOC	DOTA-D-Phe1-Tyr3-Octreotide
PET	Positron emission tomography
CECT	Contrast-enhanced CT
KPS	Karnofsky performance status
eGFR	Estimated glomerular filtration rate

Hb	Haemoglobin
WBC	White blood cell
PLT	Platelet
IV	Intravenous
SpO ₂	Saturation pulse oxygen
OSCGM	Ordered subset conjugate gradient minimiser
SLD	Sum of the longest diameters
LD	Longest diameter
SUV	Standardised uptake value
VOI	Volume-of-interest
TAD	Tumour-absorbed dose
BW	Body weight
ID	Injected dose
CI	Confidence interval

Supplementary Information

The online version contains supplementary material available at <https://doi.org/10.1186/s40658-024-00620-8>.

Additional file 1. Table S1. Details of the number of target lesions and SUV data. **Table S2.** Volume of the target lesions. **Table S3.** Ratios of tumour-absorbed doses (TADs) between PRRT cycles. **Table S4.** Correlation analyses of cycle 1 SUVs, cycle 1 TADs, and cumulative TADs with diameter change (%) without the outlier. **Table S5.** Comparisons with previous studies on the relationship between tumour-absorbed dose (TAD) and response.

Author contributions

Conceptualisation was done by Yong-il Kim and Jin-Sook Ryu. Methodology was done by Yong-il Kim and Jungsu S. Oh. Investigation was done by Sejin Ha and Yong-il Kim. Funding acquisition was done by Yong-il Kim and Jin-Sook Ryu. Formal analysis was done by Sejin ha and Yong-il Kim. Resources were done by Changhoon Yoo and Baek-Yeol Ryu. Supervision was done by Jin-Sook Ryu. Writing—original draft was done by Sejin Ha and Yong-il Kim. Writing—review and editing was done by all.

Funding

This research was supported by a grant of the Korea Health Technology R&D Project through the Korea Health Industry Development Institute (KHIDI), funded by the Ministry of Health & Welfare, Republic of Korea (Grant Number: HR18C0016). And this study was supported in part by the Asan Institute for Life Sciences, Asan Medical Center, Seoul, Korea [Grant Numbers 2021IF0022]. The funder had no role in the design, analysis, or interpretation of the study.

Availability of data and materials

The datasets generated during and/or analysed during the current study are available from the corresponding author on reasonable request.

Declarations

Ethics approval and consent to participate

This study was approved by the institutional review board of Asan Medical Center (IRB No. 2022-1581), and the requirement for informed consent was waived because of the retrospective nature of the study. This study was performed in line with the principles of the Declaration of Helsinki.

Consent for publication

Not applicable.

Competing interests

The authors declare that they have no competing interests.

Received: 25 July 2023 Accepted: 29 January 2024

Published online: 05 February 2024

References

- Shah MH, Goldner WS, Benson AB, Bergsland E, Blaszkowsky LS, Brock P, et al. Neuroendocrine and Adrenal Tumors, Version 2.2021, NCCN Clinical Practice Guidelines in Oncology. *J Natl Compr Canc Netw*. 2021;19:839–68.
- Hope TA, Bodei L, Chan JA, El-Haddad G, Fidelman N, Kunz PL, et al. NANETS/SNMMI consensus statement on patient selection and appropriate use of (177)Lu-DOTATATE Peptide Receptor Radionuclide Therapy. *J Nucl Med*. 2020;61:222–7.
- Pavel M, Öberg K, Falconi M, Krenning EP, Sundin A, Perren A, et al. Gastroenteropancreatic neuroendocrine neoplasms: ESMO Clinical Practice Guidelines for diagnosis, treatment and follow-up. *Ann Oncol*. 2020;31:844–60.

4. Pavel M, O'Toole D, Costa F, Capdevila J, Gross D, Kianmanesh R, et al. ENETS consensus guidelines update for the management of distant metastatic disease of intestinal, pancreatic, bronchial neuroendocrine neoplasms (NEN) and NEN of unknown primary site. *Neuroendocrinology*. 2016;103:172–85.
5. Ambrosini V, Kunikowska J, Baudin E, Bodei L, Bouvier C, Capdevila J, et al. Consensus on molecular imaging and theranostics in neuroendocrine neoplasms. *Eur J Cancer*. 2021;146:56–73.
6. Chalkia MT, Stefanoyiannis AP, Chatzioannou SN, Round WH, Efstathopoulos EP, Nikiforidis GC. Patient-specific dosimetry in peptide receptor radionuclide therapy: a clinical review. *Australas Phys Eng Sci Med*. 2015;38:7–22.
7. Sandström M, Garske-Román U, Granberg D, Johansson S, Widström C, Eriksson B, et al. Individualized dosimetry of kidney and bone marrow in patients undergoing ¹⁷⁷Lu-DOTA-octreotate treatment. *J Nucl Med*. 2013;54:33–41.
8. Hicks RJ, Kwekkeboom DJ, Krenning E, Bodei L, Grozinsky-Glasberg S, Arnold R, et al. ENETS consensus guidelines for the standards of care in neuroendocrine neoplasia: peptide receptor radionuclide therapy with radiolabeled somatostatin analogues. *Neuroendocrinology*. 2017;105:295–309.
9. Bruvoll R, Blakkisrud J, Mikalsen LT, Connelly J, Stokke C. Correlations between [(68)Ga]Ga-DOTA-TOC uptake and absorbed dose from [(177)Lu]Lu-DOTA-TATE. *Cancers (Basel)*. 2023;15:1134.
10. Stenvall A, Gustafsson J, Larsson E, Roth D, Sundlöf A, Jönsson L, et al. Relationships between uptake of [(68)Ga]Ga-DOTA-TATE and absorbed dose in [(177)Lu]Lu-DOTA-TATE therapy. *EJNMMI Res*. 2022;12:75.
11. Ilan E, Sandström M, Wassberg C, Sundin A, Garske-Román U, Eriksson B, et al. Dose response of pancreatic neuroendocrine tumors treated with peptide receptor radionuclide therapy using ¹⁷⁷Lu-DOTATATE. *J Nucl Med*. 2015;56:177–82.
12. Jahn U, Ilan E, Sandström M, Garske-Román U, Lubberink M, Sundin A. ¹⁷⁷Lu-DOTATATE peptide receptor radionuclide therapy: dose response in small intestinal neuroendocrine tumors. *Neuroendocrinology*. 2020;110:662–70.
13. Del Prete M, Buteau FA, Beauregard JM. Personalized (177)Lu-octreotate peptide receptor radionuclide therapy of neuroendocrine tumours: a simulation study. *Eur J Nucl Med Mol Imaging*. 2017;44:1490–500.
14. Hänscheid H, Lapa C, Buck AK, Lassmann M, Werner RA. Dose mapping after endoradiotherapy with (177)Lu-DOTATATE/DOTATOC by a single measurement after 4 days. *J Nucl Med*. 2018;59:75–81.
15. Ardenfors O, Nilsson JN, Thor D, Hindorf C. Simplified dosimetry for kidneys and tumors in (177)Lu-labeled peptide receptor radionuclide therapy. *EJNMMI Phys*. 2022;9:44.
16. Sundlöf A, Gustafsson J, Brolin G, Mortensen N, Hermann R, Bernhardt P, et al. Feasibility of simplifying renal dosimetry in (177)Lu peptide receptor radionuclide therapy. *EJNMMI Phys*. 2018;5:12.
17. Hofman MS, Lau WF, Hicks RJ. Somatostatin receptor imaging with ⁶⁸Ga DOTATATE PET/CT: clinical utility, normal patterns, pearls, and pitfalls in interpretation. *Radiographics*. 2015;35:500–16.
18. Hope TA, Abbott A, Colucci K, Bushnell DL, Gardner L, Graham WS, et al. NANETS/SNMMI procedure standard for somatostatin receptor-based peptide receptor radionuclide therapy with (177)Lu-DOTATATE. *J Nucl Med*. 2019;60:937–43.
19. Lodge MA, Wahl RL. Practical PERCIST: a simplified guide to PET response criteria in solid tumors 1.0. *Radiology*. 2016;280:576–84.
20. Eisenhauer EA, Therasse P, Bogaerts J, Schwartz LH, Sargent D, Ford R, et al. New response evaluation criteria in solid tumours: revised RECIST guideline (version 1.1). *Eur J Cancer*. 2009;45:228–47.
21. Huizing DMV, Aalbersberg EA, Versleijen MWJ, Tesselar MET, Walraven I, Lahaye MJ, et al. Early response assessment and prediction of overall survival after peptide receptor radionuclide therapy. *Cancer Imaging*. 2020;20:57.
22. Costelloe CM, Chuang HH, Madewell JE, Ueno NT. Cancer response criteria and bone metastases: RECIST 1.1, MDA and PERCIST. *J Cancer*. 2010;1:80–92.
23. Bäuerle T, Semmler W. Imaging response to systemic therapy for bone metastases. *Eur Radiol*. 2009;19:2495–507.
24. Suzuki C, Jacobsson H, Hatschek T, Torkzad MR, Bodén K, Eriksson-Alm Y, et al. Radiologic measurements of tumor response to treatment: practical approaches and limitations. *Radiographics*. 2008;28:329–44.
25. Therasse P, Arbuuck SG, Eisenhauer EA, Wanders J, Kaplan RS, Rubinstein L, et al. New guidelines to evaluate the response to treatment in solid tumors. European Organization for Research and Treatment of Cancer, National Cancer Institute of the United States, National Cancer Institute of Canada. *J Natl Cancer Inst*. 2000;92:205–16.
26. Foss CA, Plyku D, Ordonez AA, Sanchez-Bautista J, Rosenthal HB, Minn I, et al. Biodistribution and radiation dosimetry of (124)I-DPA-713, a PET radiotracer for macrophage-associated inflammation. *J Nucl Med*. 2018;59:1751–6.
27. Skovgaard D, Persson M, Brandt-Larsen M, Christensen C, Madsen J, Klausen TL, et al. Safety, dosimetry, and tumor detection ability of (68)Ga-NOTA-AE105: first-in-human study of a novel radioligand for uPAR PET imaging. *J Nucl Med*. 2017;58:379–86.
28. Lam M, Garin E, Palard-Novello X, Mahvash A, Kappadath C, Haste P, et al. Direct comparison and reproducibility of two segmentation methods for multicompartiment dosimetry: round robin study on radioembolization treatment planning in hepatocellular carcinoma. *Eur J Nucl Med Mol Imaging*. 2023. <https://doi.org/10.1007/s00259-023-06416-9>.
29. Boellaard R, Delgado-Bolton R, Oyen WJ, Giammarile F, Tatsch K, Eschner W, et al. FDG PET/CT: EANM procedure guidelines for tumour imaging: version 20. *Eur J Nucl Med Mol Imaging*. 2015;42:328–54. <https://doi.org/10.1007/s00259-014-2961-x>.
30. Akoglu H. User's guide to correlation coefficients. *Turk J Emerg Med*. 2018;18:91–3. <https://doi.org/10.1016/j.tjem.2018.08.001>.
31. Jahn U, Ilan E, Sandström M, Lubberink M, Garske-Román U, Sundin A. Peptide receptor radionuclide therapy (PRRT) with (177)Lu-DOTATATE; differences in tumor dosimetry, vascularity and lesion metrics in pancreatic and small intestinal neuroendocrine neoplasms. *Cancers (Basel)*. 2021;13:962.
32. Roth D, Gustafsson J, Warfvinge CF, Sundlöf A, Åkesson A, Tennvall J, et al. Dosimetric quantities in neuroendocrine tumors over treatment cycles with (177)Lu-DOTATATE. *J Nucl Med*. 2022;63:399–405.
33. Alipour R, Jackson P, Bressel M, Hogg A, Callahan J, Hicks RJ, et al. The relationship between tumour dosimetry, response, and overall survival in patients with unresectable Neuroendocrine Neoplasms (NEN) treated with (177)Lu DOTATATE (LuTate). *Eur J Nucl Med Mol Imaging*. 2023;50:2997–3010.

34. Malcolm JC, Falzone N, Gains JE, Aldridge MD, Mirando D, Lee BQ, et al. Impact of cyclic changes in pharmacokinetics and absorbed dose in pediatric neuroblastoma patients receiving [(177)Lu]Lu-DOTATATE. *EJNMMI Phys.* 2022;9:24.
35. Vinjamuri S, Gilbert TM, Banks M, McKane G, Maltby P, Poston G, et al. Peptide receptor radionuclide therapy with (90)Y-DOTATATE/(90)Y-DOTATOC in patients with progressive metastatic neuroendocrine tumours: assessment of response, survival and toxicity. *Br J Cancer.* 2013;108:1440–8.
36. Reccia I, Pai M, Kumar J, Spalding D, Frilling A. Tumour heterogeneity and the consequent practical challenges in the management of gastroenteropancreatic neuroendocrine neoplasms. *Cancers (Basel).* 2023;15:1861.
37. Sandström M, Freedman N, Fröss-Baron K, Kahn T, Sundin A. Kidney dosimetry in 777 patients during (177)Lu-DOTATATE therapy: aspects on extrapolations and measurement time points. *EJNMMI Phys.* 2020;7:73.
38. Padhani AR, Gogbashian A. Bony metastases: assessing response to therapy with whole-body diffusion MRI. *Cancer Imaging.* 2011;11:S129–45.
39. Sjögreen Gleisner K, Chouin N, Gabina PM, Cicone F, Gnesin S, Stokke C, et al. EANM dosimetry committee recommendations for dosimetry of 177Lu-labelled somatostatin-receptor- and PSMA-targeting ligands. *Eur J Nucl Med Mol Imaging.* 2022;49:1778–809.

Publisher's Note

Springer Nature remains neutral with regard to jurisdictional claims in published maps and institutional affiliations.